



# Targeted stimulation of active brain sources using electromagnetic reciprocity

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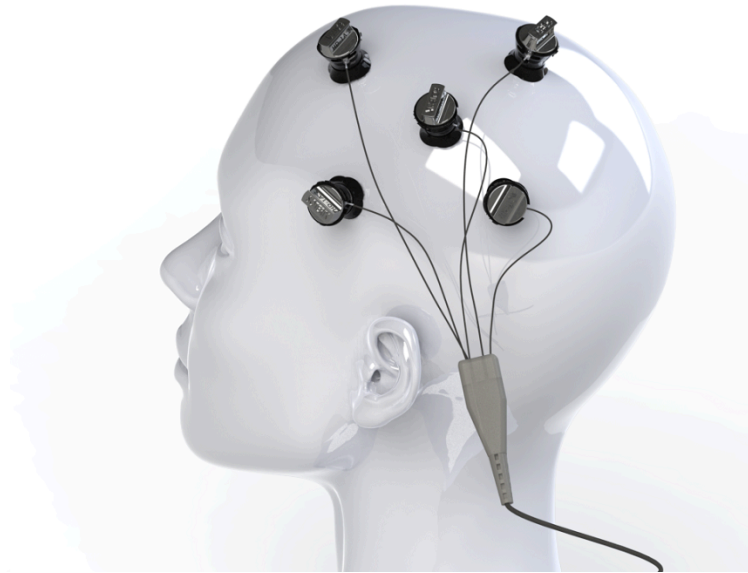
# Paradigm shift

## Conventional tDCS



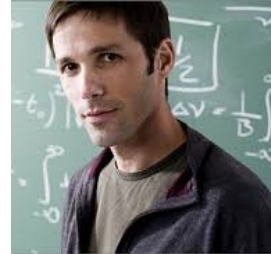
- Large pads or sponges
- Diffuse electric fields
- Optimization requires exhaustive search

## HD-tDCS

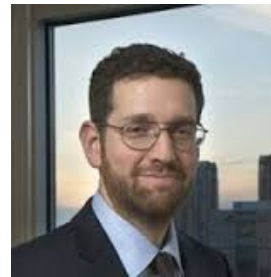


- Multiple small electrodes
- Electric field can be made focal
- Fast convex optimization steers current to target

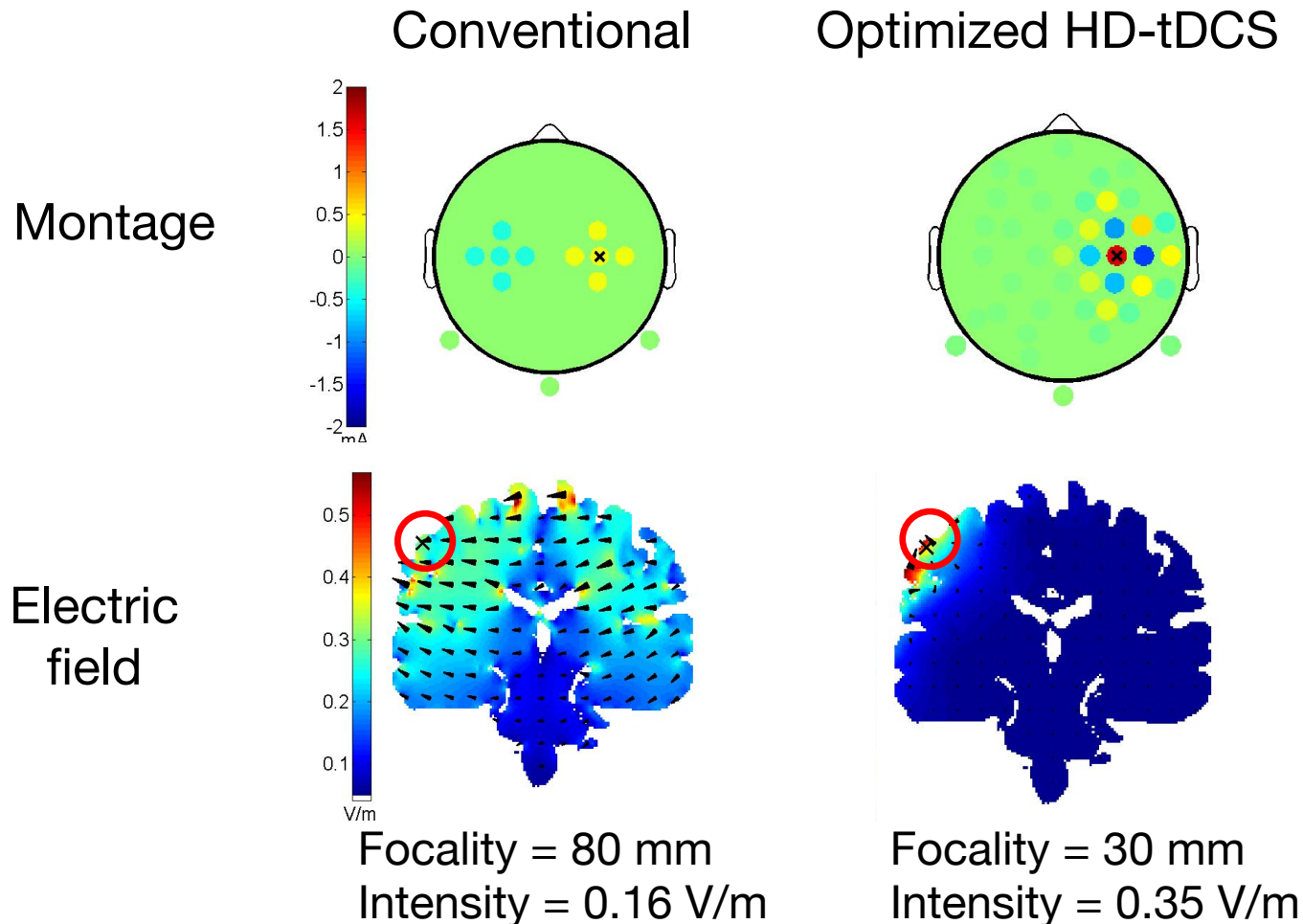
Lucas Parra



Marom Bikson

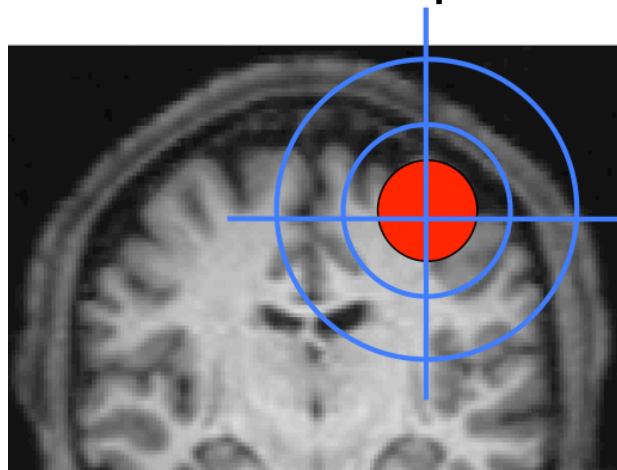


# Shaping the electric field



# Anatomical targeting

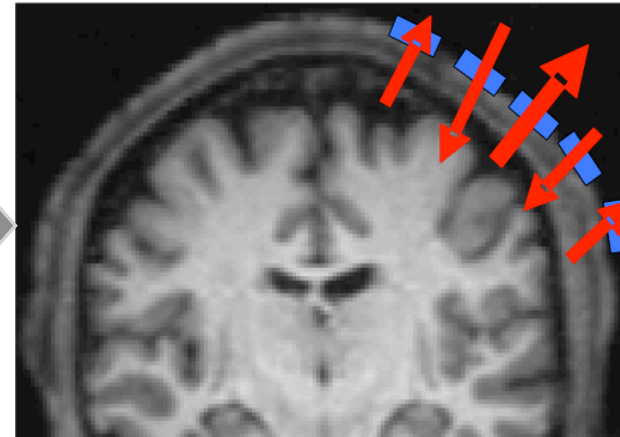
Clinician input



Algorithm

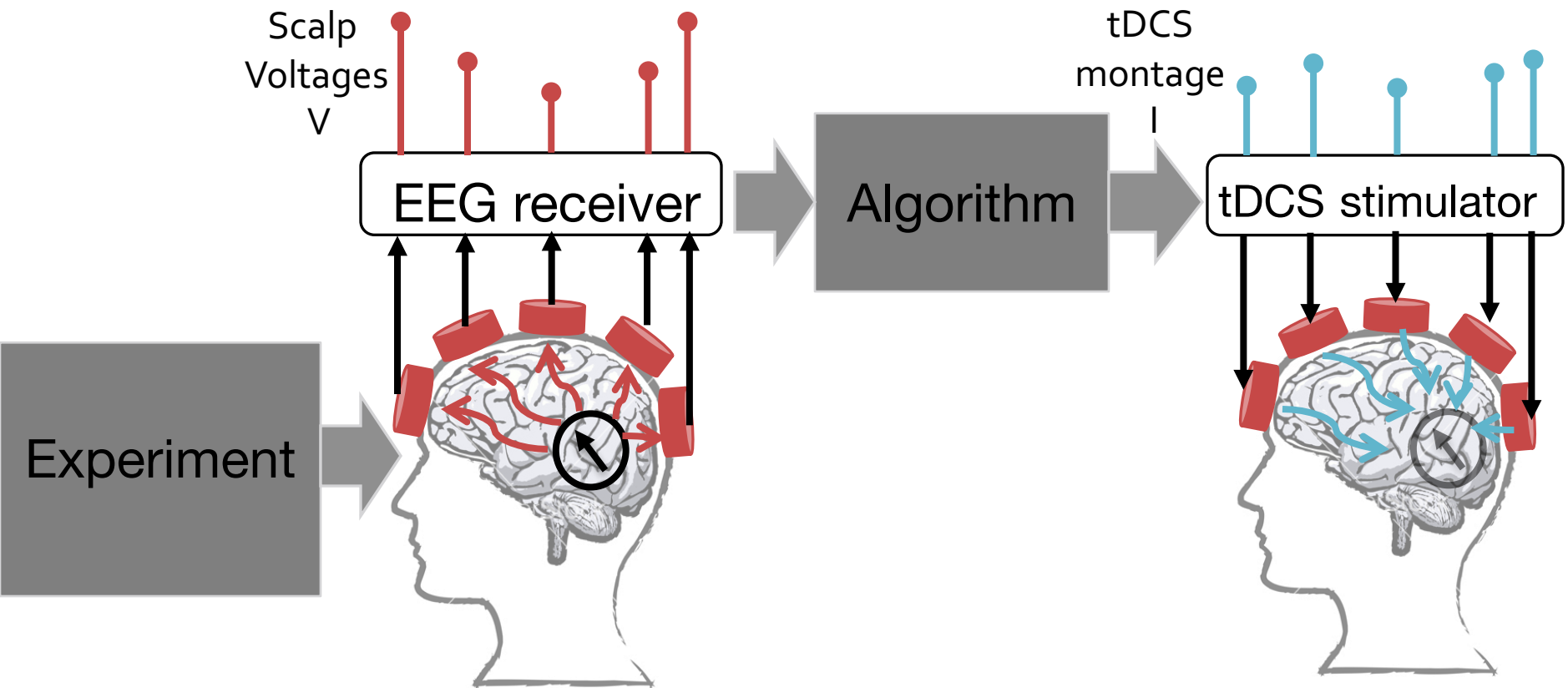


Targeted, multi-electrode stimulation

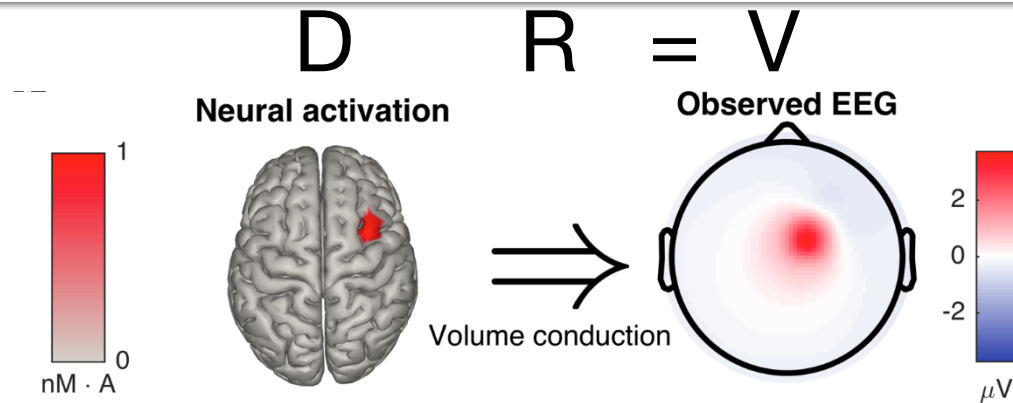


Anatomical targeting requires a “hard decision” on the required target.

# EEG-guided tDCS

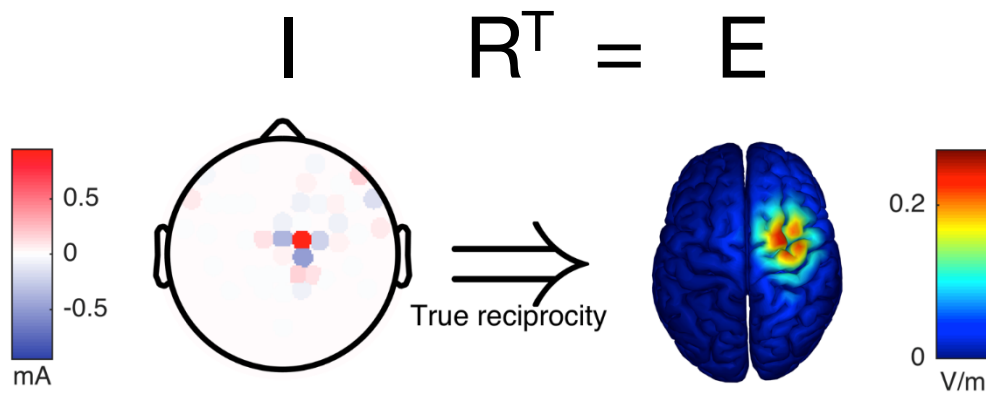


# Reciprocal tDCS in a finite element model

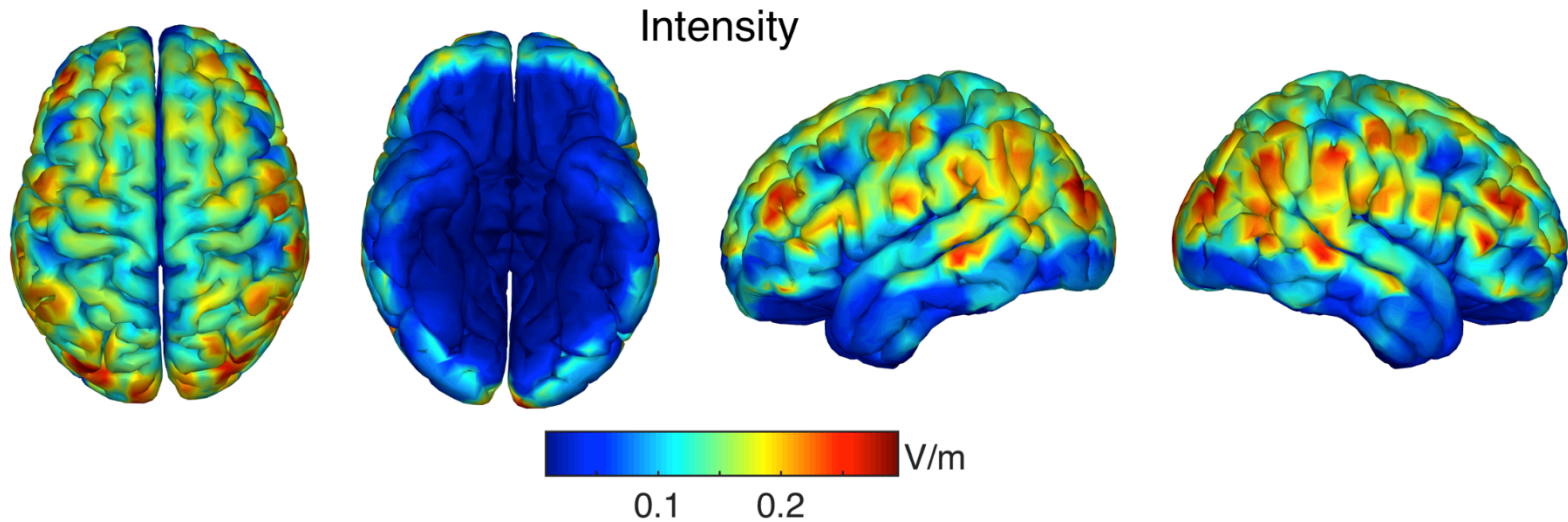
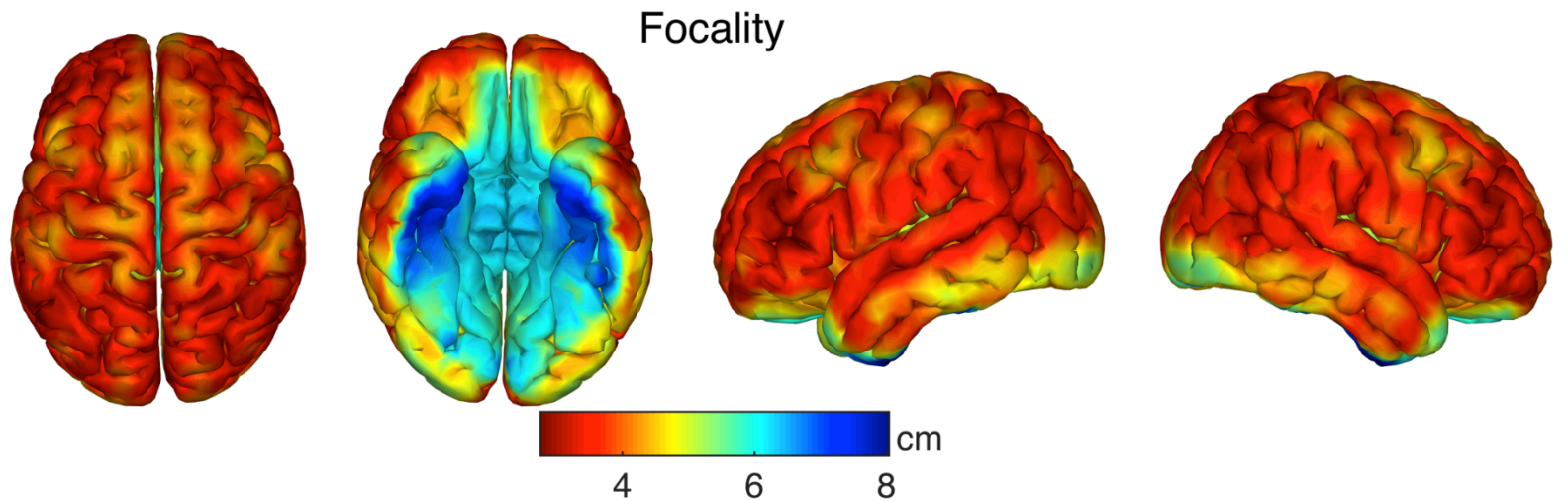


$$I = (RR^T)^{-1} V$$

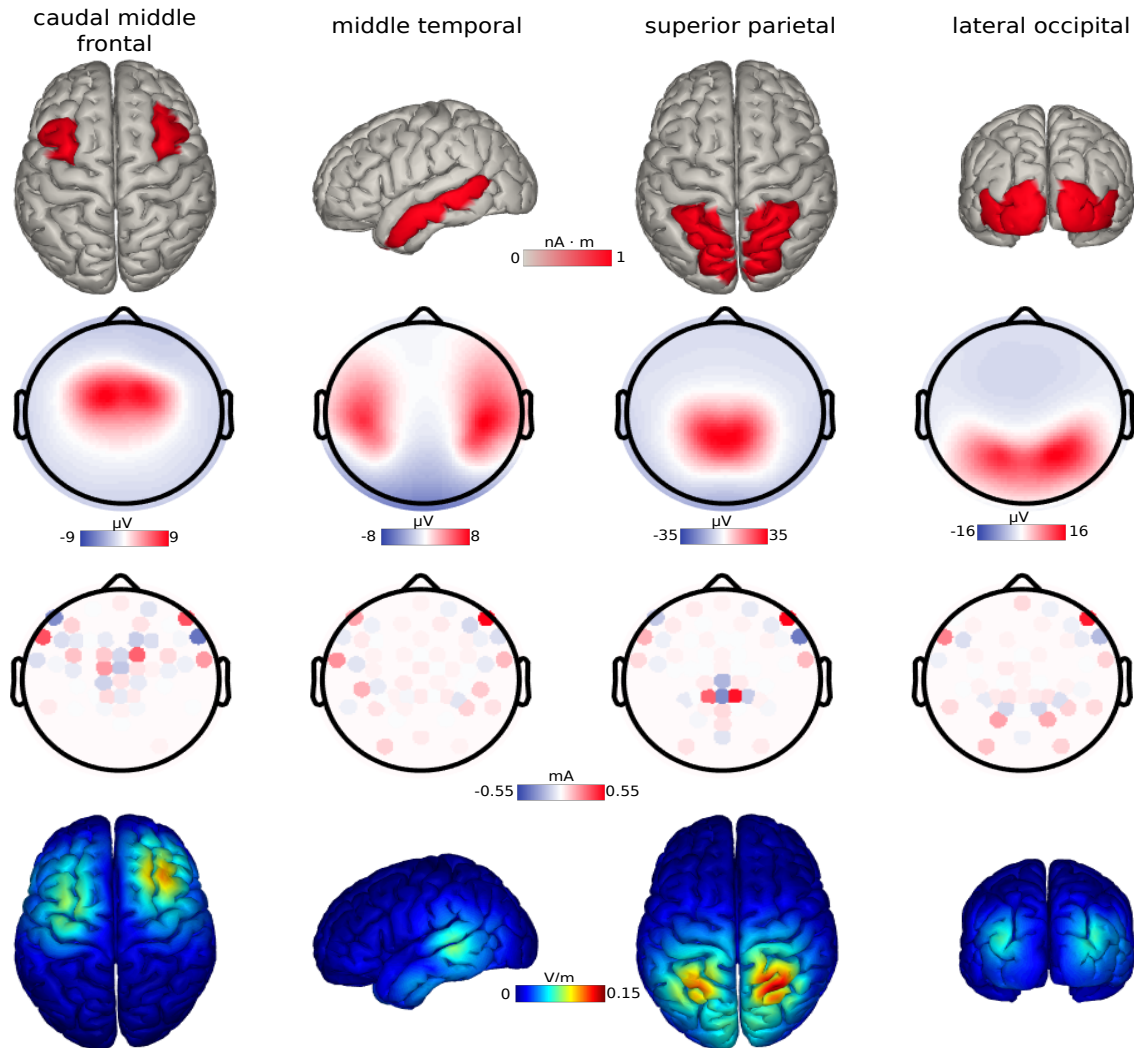
EEG-tDCS  
reciprocity solution



# Achievable focality & intensity



# Reciprocal montages are not trivial



Regions of interest

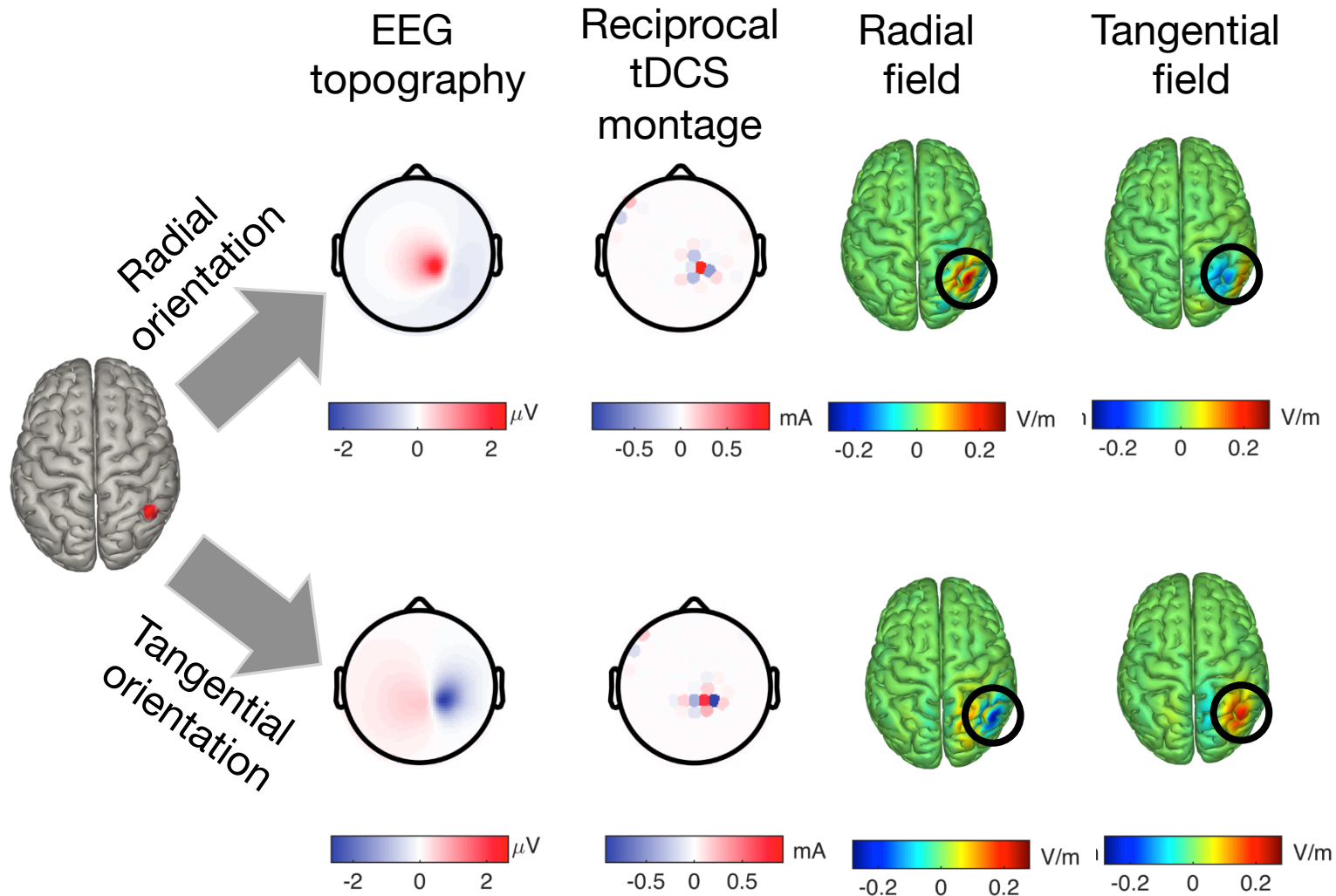
EEG topographies

Reciprocal tDCS montages

Achieved electric fields



# Reciprocity handles varying source orientation



# Takeaways

- Advantages of EEG-guided tDCS
  - Data-driven, no assumptions on target
  - Can account for **individual differences**
  - Source localization not required
  - Immediate applicability to disorders with observable EEG correlates
- Many sources of variability in tDCS
  - Electrode placement and montage could be systematized

# Acknowledgments

- Project collaborators:

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- Laurent Koessler (CRAN-Nancy)



- Marom Bikson (CCNY)

